



HOSPITAL
INNOVATIONS
Business Case: PULLUP®

Fixed loop Suspensory Fixation Devices

These original suspensory fixation devices, e.g. Endobutton®, have a fixed-loop length and whilst they are extremely popular due to their fixation strength (UTS) and stability³, they do have inherent weaknesses:

- ✗ Fixed loop devices limit the surgeon in terms of tunnel length and graft choice, and can lead to cumbersome pre-operative calculations in theatre⁴. This is particularly relevant with the recent shift towards anatomic tunnel positioning leading to smaller tunnel lengths (from traditional 45mm to between 32-36mm tunnel lengths)⁵. This in turn, with the fixed-loop design, leads to less graft in the femoral tunnel.

💡 Qi *et al.* (2011)⁶, have demonstrated that graft lengths of less than 15mm in the femoral tunnel can result in lower pull-out strength and delayed healing. With tunnel lengths as small as 32mm, there is growing concern over graft pull-out strength and healing.



Figure 2: Change in femoral tunnel lengths from longer transtibial (yellow) to shorter AM portal (red) and outside-in (blue) ACL reconstruction philosophies. Image from Osti *et al.* (2015).⁵

- ✗ 6mm over-drilling is required to flip the button, which may impact graft stability and bone tendon healing⁷.

Adjustable loop Suspensory Fixation Devices

The traditional adjustable loop fixation devices, e.g. TightRope[®] and ToggleLoc[™], were introduced to combat issues with fixed loop devices. Whilst these designs allow greater flexibility, fill the tunnel and eliminate the need for pre/intra-operative calculations³, they do not come without problems:

- ✗ Adjustable-loop suspensory fixation devices have demonstrated problems with loop lengthening after fixation, and subsequent graft displacement, loosening and surgical failure⁸.

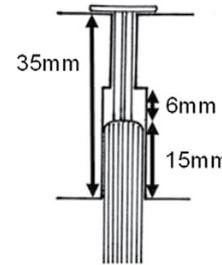


Figure : 6mm overdrilling required to flip an Endobutton. Image adapted from Eguchi *et al.* (2014).⁷

Displacement (mm)

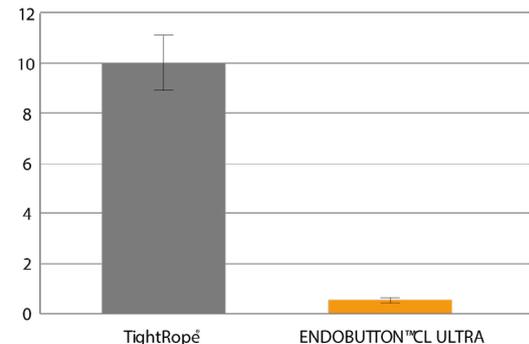


Figure 5: Average displacement for TightRope[®] and Endobutton[®] CL Ultra when loaded with a 60N static load over 10 cycles. Endobutton[®] was significantly less at 0.58mm displacement, compared to 9.95mm seen in TightRope[®]. Image adapted from Perriello, Berube and Moore (2012)⁸.

- ✗ An increased risk in elongation during the rehabilitation phase due to increased tension over a longer number of load cycles⁴.

Adjustable Suspension Fixation Loop Lengthening

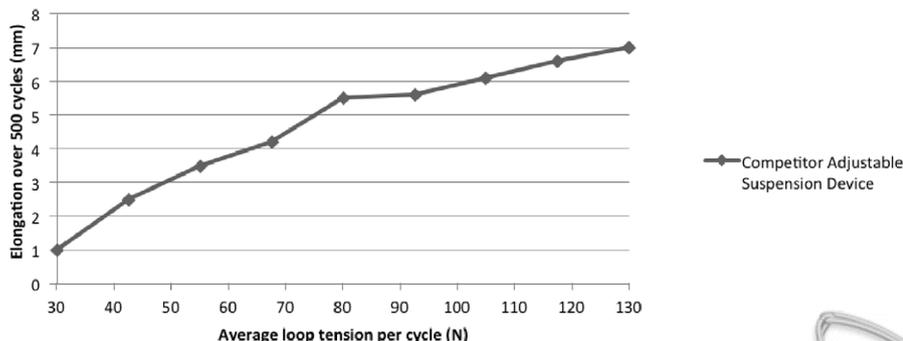


Figure 6: Increased elongation of TightRope® over 500 cycles with increasing load. Image adapted from Barrow *et al.* (2014)⁴.

- ✗ A lack of a positive flip feature which can lead to false judgment in seating of the button against the lateral cortex. On tensioning from the tibial end this can lead to slippage and graft displacement. If this isn't spotted during surgery this can also lead to graft loosening and surgical failure⁹.

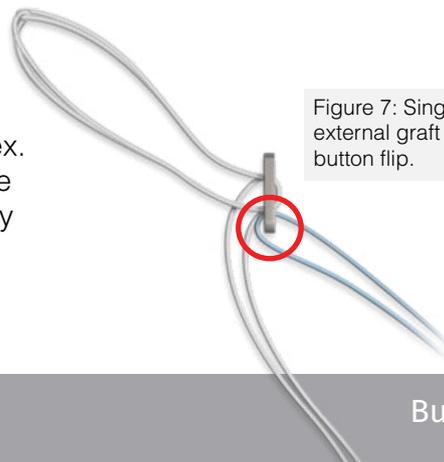
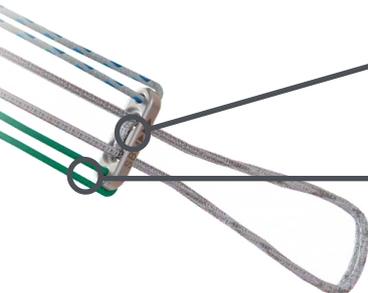


Figure 7: Single suture for external graft traction and button flip.

Designed by renowned ACL guru Dr Philippe Colombet, PULLUP® offers a novel solution, addressing concerns with both fixed loop and adjustable loop suspensory fixation devices, offering the surgeon the best of both worlds. Since 2013, 1427 PULLUP® devices have been implanted worldwide with no reported adverse events to date¹⁰.

1 Confident Stability

- Novel, patented locking mechanism with simultaneous tensioning of loop sutures eliminates slippage of graft loop during tibial fixation¹⁰
- UHMWPE central loop provides appropriate material stiffness to eliminate material stretch post-operatively seen with other competitors¹⁰
- Secondary green suture, providing a positive flip function to ensure accurate seating of the button against the femoral cortex¹⁰



• **Unique Loop-Locking System**

Chinese finger trap configuration with simultaneous tensioning of loop sutures eliminates loop lengthening and graft displacement¹⁰

• **Positive Suture Flip**

Separate flip suture ensures reliable flipping so that the button is placed securely against the cortex¹⁰

1 Confident Stability

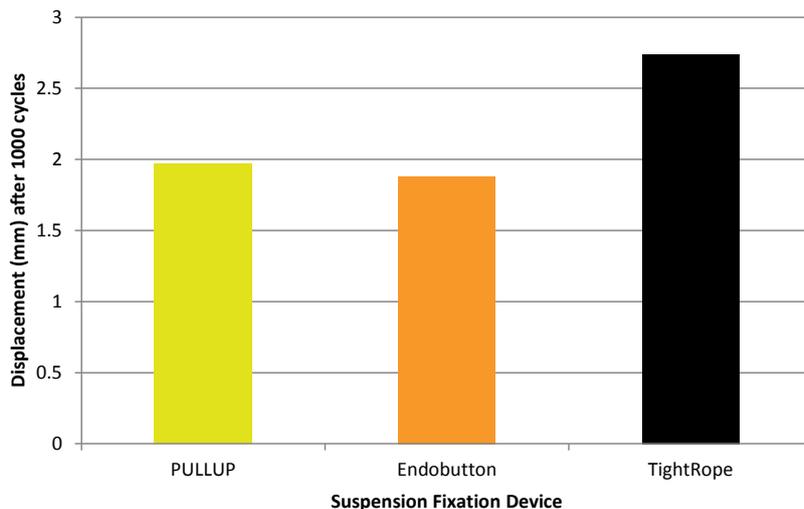


Figure 8: Graft displacement of PULLUP® and competitor suspension fixation devices after 1000 cycles in a construct. PULLUP® (1.97mm), Endobutton® (1.88mm) and TightRope® (2.74mm). TightRope® is closer to the clinical failure of 3mm displacement than both PULLUP® and Endobutton®. Data from Petre *et al.* (2012).³

Offering the best of **both**...

2 Intra-operative choice with PULLUP® adjustable loop

- Easy graft insertion eliminating the need for intra-operative calculations and limitations in tunnel and graft length choice
- Accommodates use of the same graft independent of surgical philosophy avoiding issues with shorter tunnel lengths and subsequent impact on graft length within the tunnel when using fixed loop devices
- Bone preserving: PULLUP® fills the tunnel with tendon graft avoiding concerns on over-drilling, graft stability and bone-tendon healing



Adjustable Loop System
Allows for surgeon flexibility and eliminates the need to plan intra-operatively

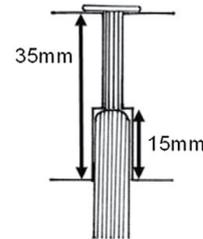


Figure 6: PULLUP® allows complete tunnel filling with the tendon graft, avoiding concerns on graft stability and healing. Image adapted from Eguchi *et al.* (2014)⁷.

Stability and **Choice**

Traditional adjustable loop suspensory fixation
Loop Lengthening - Petre, B *et al.* (2012)³

Study Objective:

To assess and compare the fixation strength of 4 common cortical suspension fixation devices; S&N Endobutton® CL, Arthrex TightRope RT®, Biomet ToggleLoc™ and Conmed XO Button™.

Methodology:

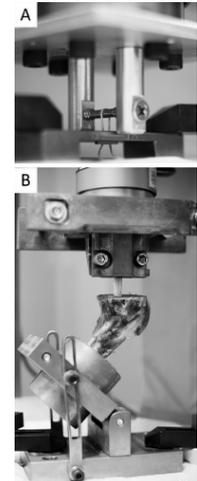
All four devices were tested under both cyclic and pull-to-failure conditions using a tensile testing machine. The devices were tested in a device-only construct (a) and a bone-device-tendon construct (B) in porcine femurs.

Results:

3.00mm is the displacement threshold defined as a clinical failure. ToggleLoc™ exceeded the 3.00mm threshold, whilst TightRope® came close at 2.74mm.

Conclusion:

- Graft displacement of up to 3.34mm was seen in adjustable loop fixation devices close to the clinical failure threshold. However, PULLUP® overcomes this with a novel loop locking system, with comparable displacement to Endobutton®.



	Cyclic displacement after 1000 cycles (mm)
Endobutton®	1.88
TightRope®	2.74
ToggleLoc™	3.34
XO Button™	1.82

Limitations with fixed loop suspensory devices Shorter Tunnels - Osti, M *et al.* (2015)⁵

Study Objective:

To evaluate the bone tunnel parameters of three different surgical techniques: AM portal (AMP), outside-in (OI), and the traditional transtibial (TT) approach.

Methodology:

The study included 36 patients (TT technique), 32 (AMP) and 32 (OI). CT scans were used to measure characteristics of the femoral bone tunnels.

Results:

Both AMP and OI techniques resulted in a more precise replication of tunnel depth and height, leading to a more native ACL attachment site. As a consequence surgeons are more inclined to use these modern techniques.

	Transtibial	AM Portal	Outside-In
Tunnel Length (mm)	42.31	33.35	35.58

Conclusion:

- A move toward a more anatomic approach for tunnel positioning has led to smaller femoral tunnels resulting in reduced graft length within the femur. For example, fixed loop suspension fixation devices with a loop length of 20mm would lead to as little as 13mm of graft in the femoral tunnel.



- Qi *et al.* (2011)⁶ have demonstrated that graft lengths of less than 15mm can result in lower pull-out strength and delayed healing.

Technical Specification



PULLUP®	Technical Parameters
Composition Plate Braid Pull & flip sutures	Titanium Ultra High Molecular Weight Polyethylene (UHMWPE) Polyester (PE)
Ultimate tensile strength	823N (up to 600N required for post-op rehabilitation)
Stiffness	199N/mm (Endobutton=201N/mm, TightRope=208N/mm)
Loop elongation on cyclic loading	1.97mm (Endobutton=1.88mm, TightRope=2.74mm)
Loop length	40mm
Loop braid diameter	1mm (USP 8-0)
Pull & flip suture diameter	0.7mm (USP 5-0)
Pull suture strength	500N
Flip suture strength	250N
MRI Compatibility	Yes
CE classification	IIb (93/42/CEE Directive)

1. Millennium Medical Technology Report: European Markets 2010.
2. UK National Ligament Registry Data.
3. Petre, B. *et al.* (2012). Femoral Cortical Suspension Devices for Soft Tissue Anterior Cruciate Ligament Reconstruction: A Comparative Biomechanical Study. 41(2): 416-422.
4. Barrow, A. *et al.* (2014). Femoral Suspension Devices for Anterior Cruciate Ligament Reconstruction: Do Adjustable Loops Lengthen?. *The American Journal of Sports Medicine*. 42(2): 343-349.
5. Osti, M. *et al.* (2015). Femoral and Tibial Graft Tunnel Parameters After Transtibial, Anteromedial Portal and Outside-In Single-Bundle Anterior Cruciate Ligament Reconstruction. *The American Journal of Sports Medicine*. Advanced Online Publication. Retrieved from: <http://www.ncbi.nlm.nih.gov/pubmed/26138734>.
6. Qi, L., Chang, C., Jian, L. Xin, T. and Gang, Z. (2011). Effect of Varying the Length of Soft-tissue grafts in the Tibial Tunnel in a Canine Anterior Cruciate Ligament Reconstruction Model. *Arthroscopy*. 27(6):825-833.
7. Eguchi, A. *et al.* (2014). Mechanical Properties of Suspensory Fixation Devices for Anterior Cruciate Ligament Reconstruction: Comparison of the Fixed-Length Loop Device Versus the Adjustable-Length Loop Device. *The Knee*. 21: 743-748.
8. Perriello, M., Berube, R. and Moore, C. (2012). Displacement of a Fixed Versus Adjustable Suspensory Fixation Device for Anterior Cruciate Ligament Reconstruction. *Bone and Joint Science*. 3(7):1-4.
9. Nag, H. L. and Gupta, H. (2012). Seating of TightRope RT Button Under Direct Arthroscopic Visualisation in Anterior Cruciate Ligament Reconstruction to Prevent Potential Complications. *Arthroscopy Techniques*. 1(1): e83-e85.
10. Data on file at SBM.



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